Dosimetric study of SIB-IMRT versus SIB-3DCRT for breast cancer with breath-hold gated technique

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Original Article

Abstract

Background and purpose: 3-dimensional conformal therapy (3DCRT) is widely employed radiation therapy technique for breast cancer, but there is still need to minimize the doses to organ at risk (OAR) using 3DCRT. A few clinical studies have discussed using intensity modulated radiation therapy (IMRT) to address this shortfall. Simultaneous integrated boost (SIB) has been used in head and neck and prostate cancer, and there is a growing interest in using SIB for breast cancer too. This study aimed to compare SIB-IMRT versus SIB-3DCRT for breast cancer patients. Materials and Methods: SIB-3DCRT treatment plans were created for 36 consecutive patients. Dose was prescribed as 45 Gy in 25 fractions to the planning target volume (PTV)-1 and 60 Gy in 25 fractions to PTV-2. Treatment plans were normalized to 95% of PTV volume receiving 95% of the prescription dose. The conformity index (CI), homogeneity index (HI), lung dose, heart dose, left anterior descending artery (LAD) dose, and low dose volume and integral dose of normal healthy tissue were recorded and analyzed. Results: With the use of IMRT technique, there was an improvement in CI (0.14) when compared to CI of 3DCRT (0.18; p = 0.01). However, there was no significant difference in the HI (p = 0.45). On average, the V20Gy of ipsilateral lung was 37.9% for 3DCRT and 22.4% (p < 0.01) for IMRT, whereas the V20Gy of total lung (ipsilateral + contralateral) was 21.8% for 3DCRT and 12.14 (p < 0.01) for IMRT. Similarly, average V40Gy of heart was 7.5% for 3DCRT and 2.13 % (p = 0.01) for IMRT. The LAD maximum dose to left side breast patients, on average, was 39.5 Gy for 3DCRT and 29.17 Gy (p = 0.03) for IMRT. The average number of monitor units was about 180 for 3DCRT and 1441 (p < 0.01) for IMRT. Conclusion: IMRT for breast cancer treatment is feasible. In comparison to 3DCRT, IMRT can reduce the maximum dose to the target volume, and dose to the OAR. However, 3DCRT technique is superior in terms of low dose volume, integral dose, and treatment time. With the use of breath-hold gated technique in IMRT, it can further improve the target coverage and reduction of doses to the heart, lung, and LAD. SIB technique could reduce the overall treatment duration by about one week.

Keywords: Intensity Modulated Radiation Therapy, Three Dimensional Conformal Radiotherapy, Simultaneous Integrated Boost, Breath-Hold, Technique, Breast Cancer

Introduction

Breast cancer is the most common malignancy in women. Radiotherapy is an integral part of breast cancer management either in breast conservation surgery (BCS) or in post mastectomy cases. Many prospective studies have shown that adjuvant radiotherapy improves local control and survival rate in breast cancer patients after surgery.¹ During earlier days of radiotherapy, opposed wedged fields with half beam block was considered as the standard radiation therapy technique. In the last decade, an introduction of linear accelerators has made 3-dimensional conformal radiotherapy (3DCRT) as a standard treatment technique, which can reduce the doses to the lung, heart, and other critical structure doses in the breast cancer treatment. However, using 3DCRT, it is not always possible to achieve adequate normal tissue sparing, especially when treating left side chest wall patients. This is mainly due to overlying concave shape of

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the target, which can result more doses to adjacent structures such as heart and lung. Hong et al.² compared intensity modulated radiation therapy (IMRT) with 3D conformal tangential wedged beams, and showed the reduction of dose to the coronary arteries, contra lateral breast, ipsilateral lung, and surrounding soft tissues using IMRT. By modulating photon beam, it is possible to obtain concave and convex shape dose distributions with IMRT, and it has the ability to conform radiation dose to irregular target volumes sparing the underlying critical structures resulting in better tumor control probability (TCP) and reduced normal tissue complication probability (NTCP). The main purpose of this study was to further evaluate normal tissue sparing and dosimetric analysis of simultaneous integrated boost (SIB)-3DCRT and SIB-IMRT in breast patients, with focus on breath-hold gated technique.

Materials and Methods

In this retrospective treatment planning study, we used computed tomography (CT) data of 36 consecutive patients with breast cancer post lumpectomy (18 left sides and 18 right sides), and all patients were treated with respiratory gated technique for breast radiotherapy.

CT Simulation

All 36 patients were simulated using 4D CT scanner (Philips Medical Systems, Andover, MA, USA) with whole-body Vaclok (Civco Medical Solutions, Iowa, USA) immobilization system. Patients were positioned on a wide bore CT-SIM couch with the help of lasers, and both arms of the patient were raised above patient’s head. Furthermore, radio opaque markers were placed during the immobilization procedure to guide the isocenter shift. For all the patients, CT scans images were obtained from mandible to upper abdomen area with intravenous contrast, and CT scans were obtained using slice thickness of 5 mm. Prior to CT simulation, patients were given training on breath-hold technique.

Target Delineation and Dose Prescription

After the CT simulation, the Digital Imaging and Communications in Medicine (DICOM) images were transferred to Eclipse treatment planning system (TPS) (version 10.0.34, Varian Medical Systems, Palo Alto, California, USA). Clinical target volume (CTV), planning target volume (PTV) and Organ at Risk (OAR) volumes were delineated on the axial CT slices. The lumpectomy gross tumor volume (L-GTV) was contoured using all available clinical and radiographic information including the excision cavity volume, architectural distortion, lumpectomy scar, seroma and/or extent of surgical clips.

CTV1 included the palpable breast tissue demarcated with radio opaque markers at CT simulation. The apparent CT glandular breast tissue visualized by CT, consensus definitions of anatomical borders, and the lumpectomy CTV from the RTOG breast cancer atlas. The breast CTV is limited anteriorly within 3 mm from the skin and posteriorly to the anterior surface of the pectoralis, serratus anterior muscle excluding chest wall. PTV was created by 3D expansion of CTV1 by 7 mm. CTV2 was created by 1 cm 3D expansion from L-GTV and was limited posteriorly at anterior surface of the pectoralis and antero-laterally 3 mm from skin. PTV2 was created by 7 mm 3D expansion of CTV2. The normal structures were contoured as ipsilateral lung, contra lateral lung, contra lateral breast, heart, left anterior descending (LAD) artery, spinal cord, esophagus, trachea, humerus head, and liver. Dose prescription was applied per International Commission on Radiological Units and Measurements (ICRU) 50 and 62. Specifically, dose was prescribed as 45 Gy in 25 fractions (1.8Gy/fraction) to the PTV-1 and 60 Gy in 25 fractions (2.4Gy/fraction) to PTV-2.

Treatment planning

For treatment planning, 6 mega-voltage (MV) X-rays from Clinac 600CD linear accelerator (Varian Medical Systems, Palo Alto, California, USA) integrated with 120 leaves millennium multi-leaf collimator (MLC) was used. For the dynamic IMRT plans, 7 non-coplanar beams were used to achieve the minimum criteria of 95% of the volume received 95% of the prescribed dose. The treatment fields were almost evenly spaced within an arc of 180° on the side of the tumor. Gantry angles ranged from 330° to 150° (clockwise) for the left side tumors and from 50° to 210° (counterclockwise) for the right side tumors. In Eclipse TPS, the IMRT plans were created with inverse plan optimization, and the algorithm used was Dose Volume Optimizer (version 10.0.28). For the dose calculation, pencil beam convolution (PBC) algorithm (version 10.0.28) was used, and leaf motions were calculated with leaf motion calculator (LMC) algorithm (version 10.0.28). Heterogeneity correction was done using modified Batho method in the Eclipse. For plan optimization, OAR dose constraints were given as ipsilateral lung V₂₀ < 30 %, heart V₅₀, V₆₀, and mean dose as low as possible, contra-lateral breast mean dose less than 5 Gy, and spinal cord maximum point dose less than 40 Gy. For the 3DCRT plans, 4 to 6 non-coplanar beams were used to produce adequate dose coverage for the PTV. Critical organs were shielded using MLC without compromising PTV coverage. Beam weights were adjusted until the optimum coverage and acceptable hot spots were achieved. Additionally, field-in-field was created to reduce hotspot equal to or lower than 110% as well as to improve the target coverage and homogenous dose distribution in the PTV.

Plan evaluation

Dose-Volume Histograms (DVH) was used to analyze the volume receiving 20 Gy, 30 Gy and 40 Gy, mean, maximum and minimum doses. The target dose uniformity and conformity were calculated and evaluated. Different scoring indices were given by various authors. In this study, we have followed indices defined by ICRU 83.
The conformity index (CI) as defined in ICRU 83 is

\[ \text{CI} = \frac{\text{Volume of PTV covered by the reference dose}}{\text{Volume of PTV}} \]  
Eq. 1

CI = 1.0 is ideal value

The Homogeneity Index (HI) as defined in ICRU 83 is

\[ \text{HI} = \frac{D_{50\%} - D_{95\%}}{D_{50\%}} \]  
Eq. 2

Where, \( D_{2\%}, D_{98\%}, D_{50\%} \) is dose received by 2%, 98%, 50% volume. HI = 0 (Zero) is ideal value. Also, to illustrate the low dose volume effect, \( V_{50\%} \) volume and integral dose were calculated for normal healthy tissue.

Integral Dose = Mean Dose (Gy) x Volume (Cm³)  
Eq. 3

### Statistical Analysis

Statistical Analysis was performed using the Wilcoxon Signed Rank test. This matched pair t test was applied to determine the statistical difference between the dose–volume data for IMRT versus 3DCRT. The values are reported in ranges. The reported p value is two tailed, and p values of < 0.05 are considered statistically significant.

### Results and Discussion

Dose volume histograms of the normal tissues of both the plans (IMRT and 3DCRT) are presented in Table 1. The normalized target coverage of both treatment methods is presented in Table 2 and Table 4. The PTV mean dose for 3DCRT is 47.10 Gy compared to 45.88 Gy (p < 0.01) with IMRT. The dose distribution in axial sections is shown in Figures 1 and 2. These axial sections clearly show that con- 
cave PTV coverage and exclusion of LAD during optimiza-
tion by IMRT. Also, previous studies have reported lower doses to the ipsilateral lung, contra lateral lung, contra lateral breast, heart, and LAD doses using IMRT technique.\(^{10,11}\)

3D conformal plans using asymmetric jaw and field-in-field technique provides better coverage than a conventional physical wedged –half beam blocked or physical wedged-asymmetric fields. Furthermore, physical wedge has limitation in field width and lengths. With 3DCRT, the hot spots occurred in superficial skin surface, but IMRT exhibited better control in shifting the hot spots, with a possibility of keeping dose to the skin equal to or less than the prescription dose.

#### Dose homogeneity and conformity

The use of equally spaced gantry angles improved homogeneity and conformity indices as well as reduced the volume of critical normal tissues such as the heart and ipsilateral lung receiving a high dose as shown by Hong et al.\(^2\). In this study, we used equally spaced beam angles for both the IMRT and 3DCRT plans, and the average target maximum dose was lower with IMRT; however, it was not statistically significant. Although the mean breast volume in our study was 1221 cc, which is relatively higher compared to the literature\(^12\), we were able to demonstrate optimized coverage and reduced dose to the critical organs.

The inverse–planning IMRT further reduced hotspots mainly due to beam modulation during optimization compared to 3DCRT, where beam modulation is not available. Previous planning studies\(^13,14\) with multiple fields showed the PTV-95% coverage values ranging from 90% to 97 %, whereas all our optimized plans had the PTV-95% coverage values of >95% of prescription dose. With the use of IMRT technique, our data showed that there is a consistent improvement in conformity index from 0.18 for 3DCRT to 0.15 for IMRT (p=0.01). However, there was no significant difference (\( p = 0.45 \)) when HI of 3DCRT was compared to that of IMRT.

### Table 1: Comparison of normal tissue dose volume parameters for Respiratory Gated IMRT and 3DCRT breast cancer patients (Statistics based on Wilcoxon Signed Rank Test). The values are averaged over 36 analyzed patients.

<table>
<thead>
<tr>
<th>Organ</th>
<th>Parameter</th>
<th>SIB-3DCRT</th>
<th>SIB-IMRT</th>
</tr>
</thead>
<tbody>
<tr>
<td>Ipsilateral lung</td>
<td>V(_{30%} ) (%)</td>
<td>37.9</td>
<td>22.4</td>
</tr>
<tr>
<td></td>
<td>V(_{50%} ) (%)</td>
<td>32.24</td>
<td>16.08</td>
</tr>
<tr>
<td>Heart</td>
<td>Mean (Gy)</td>
<td>20.29</td>
<td>16.51</td>
</tr>
<tr>
<td>Both Lung</td>
<td>V(_{50%} ) (%)</td>
<td>7.5</td>
<td>2.13</td>
</tr>
<tr>
<td>LAD</td>
<td>Max. Dose (Gy)</td>
<td>21.8</td>
<td>12.14</td>
</tr>
</tbody>
</table>

### Table 2: Comparison of planning target volume (PTV1) coverage parameter for Respiratory Gated IMRT and 3DCRT breast cancer patients (Statistics based on Wilcoxon Signed Rank Test). The values are averaged over 36 analyzed patients.

<table>
<thead>
<tr>
<th>PTV 1 Parameter</th>
<th>SIB-3DCRT</th>
<th>SIB-IMRT</th>
<th>p</th>
</tr>
</thead>
<tbody>
<tr>
<td>Minimum Dose (Gy)</td>
<td>24.07</td>
<td>32.03</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Maximum Dose (Gy)</td>
<td>51.97</td>
<td>59.68</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Coverage (%)</td>
<td>96.8</td>
<td>98.22</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Conformity Index</td>
<td>0.18</td>
<td>0.14</td>
<td>0.01</td>
</tr>
<tr>
<td>Homogeneity Index</td>
<td>1.03</td>
<td>1.01</td>
<td>0.45</td>
</tr>
<tr>
<td>Mean Dose (Gy)</td>
<td>47.16</td>
<td>45.88</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Mod Dose (Gy)</td>
<td>49.12</td>
<td>48.92</td>
<td>0.32</td>
</tr>
<tr>
<td>Median Dose (Gy)</td>
<td>50.5</td>
<td>48.8</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Stnd. Deviation(Gy)</td>
<td>6.35</td>
<td>4.17</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>V(_{50%} ) (%)</td>
<td>48.69</td>
<td>29.83</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>V(_{50%} ) (%)</td>
<td>30.7</td>
<td>11.29</td>
<td>&lt;0.01</td>
</tr>
</tbody>
</table>
In patients with breast cancer, it is intended that the irradiated heart volume be minimized to the greatest possible degree without compromising the target coverage. The risk of pericardial events is probably related to both dose and volume of radiation. The incidences of pericardial disease decrease with the use of sub cranial blocking the major vessels at 30 Gy. Stewart et al. concluded that the dose should be limited to 60 Gy for less than 25% of cardiac volume and 45 Gy for more than 65% of cardiac volume.

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In our study the heart V_{50Gy} was significantly lower in IMRT than in 3DCRT (p < 0.01), especially for left sided breast cancer patients, with mean heart V_{50Gy} of 7.5% for 3DCRT versus IMRT as 2.13% (p = 0.01). Gagliardi et al. reported that CAD risk was much reduced at doses less than 30 Gy. Mean values of V_{50Gy} were <5% for IMRT compared with studies reporting V_{50Gy} values in the range of 2% to 5%. Increased cardiac mortality risk associated with left side breast patients in the long term was reported by multiple authors. The advancement in treatment techniques such as IMRT has enabled to reduce cardiac exposure, and steady decline of radiation risk is being noticed. Furthermore, Boivin et al. noted that the anteriorly placed coronary arteries were more often affected by radiation therapy (compared with the circumflex artery). In our study, mean LAD maximum dose was 39.5 Gy for 3DCRT and 29.17 Gy for IMRT (p = 0.03).

**Lung dose**

The occurrence of radiation pneumonitis (RP) is related to the ipsilateral lung volume irradiated. In our study, the ipsilateral lung V_{20Gy} for IMRT (22.4%) is significantly less than that for 3DCRT (37.9%; p < 0.01). Ipsilateral lung mean dose was also higher in 3DCRT (20.29 Gy) compared to the one in IMRT (16.51Gy) (p < 0.01). Both the lung V_{50Gy} and

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**TABLE 3:** Comparison of MU, ID and V5 parameter for Respiratory Gated IMRT and 3DCRT breast cancer patients (Statistics based on Wilcoxon Signed Rank Test). The values are averaged over 36 analyzed patients.

<table>
<thead>
<tr>
<th>Parameter</th>
<th>SIB-3DCRT</th>
<th>SIB-IMRT</th>
<th>p</th>
</tr>
</thead>
<tbody>
<tr>
<td>Monitor Units</td>
<td>180</td>
<td>1441</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Integral Dose (Gy-Cm³)</td>
<td>145210</td>
<td>197428</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>V_{50Gy} (%)</td>
<td>18.89</td>
<td>30.61</td>
<td>&lt;0.01</td>
</tr>
</tbody>
</table>

**TABLE 4:** Comparison of planning target volume (PTV2) coverage parameter for Respiratory Gated IMRT and 3DCRT breast cancer patients (Statistics based on Wilcoxon Signed Rank Test). The values are averaged over 36 analyzed patients.

<table>
<thead>
<tr>
<th>PTV 2 Parameter</th>
<th>SIB-3DCRT</th>
<th>SIB-IMRT</th>
<th>p</th>
</tr>
</thead>
<tbody>
<tr>
<td>Minimum Dose (Gy)</td>
<td>56.41</td>
<td>53.9</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Maximum Dose (Gy)</td>
<td>64.9</td>
<td>64.01</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Coverage (%)</td>
<td>98.3</td>
<td>99.77</td>
<td>0.13</td>
</tr>
<tr>
<td>Conformity Index</td>
<td>0.12</td>
<td>0.08</td>
<td>0.01</td>
</tr>
<tr>
<td>Homogeneity Index</td>
<td>1.02</td>
<td>1.01</td>
<td>0.11</td>
</tr>
<tr>
<td>Mean Dose (Gy)</td>
<td>61.1</td>
<td>61.72</td>
<td>0.13</td>
</tr>
<tr>
<td>Mod Dose (Gy)</td>
<td>61.17</td>
<td>62.13</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Median Dose (Gy)</td>
<td>61.99</td>
<td>62.45</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Stnd. Deviation(Gy)</td>
<td>1.5</td>
<td>1.21</td>
<td>0.01</td>
</tr>
</tbody>
</table>

**TABLE 5:** Comparison of Non-Gated IMRT with respiratory Gated IMRT (mean) breast cancer patients (Statistics based on Wilcoxon Signed Rank Test). The values are averaged over 36 analyzed patients.

<table>
<thead>
<tr>
<th>Parameters</th>
<th>Non-Gated SIB-IMRT</th>
<th>Gated SIB-IMRT</th>
<th>p</th>
</tr>
</thead>
<tbody>
<tr>
<td>LAD-Maximum Dose</td>
<td>35.62 Gy</td>
<td>29.17 Gy</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Heart-V_{30Gy}</td>
<td>9.27 %</td>
<td>5.91 %</td>
<td>&lt;0.01</td>
</tr>
<tr>
<td>Ipsilateral Lung-V_{30Gy}</td>
<td>30.2 %</td>
<td>22.4 %</td>
<td>0.03</td>
</tr>
<tr>
<td>PTV -95% of prescription</td>
<td>96.81%</td>
<td>98.22 %</td>
<td>&lt;0.01</td>
</tr>
</tbody>
</table>

In patients with breast cancer, it is intended that the irradiated heart volume be minimized to the greatest possible degree without compromising the target coverage. The risk of pericardial events is probably related to both dose and volume of radiation. The incidences of pericardial disease decrease with the use of sub cranial blocking the major vessels at 30 Gy. Stewart et al. concluded that the dose should be limited to 60 Gy for less than 25% of cardiac volume and 45 Gy for more than 65% of cardiac volume.

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mean dose were significantly lower in IMRT than in 3DCRT (p < 0.01). Contra lateral lung V50G and mean dose of both the plans showed no significant differences. The mean lung doses (MLD) of both lung were higher compared to the report from Marks et al23, and this may be due to larger breast volumes in our study. Since there is no absolute safe MLD below which there is no pneumonitis, the clinically accepta-
ble risk of RP depends on the risk-benefit ratio of the individual patient selection basis.

Secondary malignancy
The IMRT plans contributed a modestly higher dose to adja-
cent healthy soft tissues. In our study, the mean V50G volume for 3DCRT was much lower than that of IMRT. The main concern with healthy tissue dose increases of this magnitude is an increased risk of late second malignancy.24, 25 Some investigators suggest that IMRT might increase the incidence of secondary cancer from 1% in conventional planning to 1.75% in IMRT planning for patient’s surviving 10 years.24

Furthermore, the treatment Monitor Unit (MU) was signifi-
cantly higher in IMRT technique. The monitor unit for IMRT is 6-8 times more than 3DCRT is a concern.24, 26, 27 This in turn shows that the integral dose would be higher. Pirzkall et al.28 studied that the integral dose for IMRT was higher than conventional treatment. Similar observation was made in our study as integral dose for IMRT was 22% higher than that for 3DCRT. This higher integral dose was probably due to increased number of beams used in IMRT than in 3D CRT, thus involving larger volume of healthy tissue during IMRT plan optimization. Modulation of beams also increases the treatment time during treatment delivery. Furthermore, the leakage and scatter dose to non-target tissue of the patients will be proportional to the number of monitor units used. Few studies 13, 29 have found to have increased low dose volumes with increasing beam angles.

High integral dose attributed to second malignancy, which is likely to be of greatest concern in younger women and in patients with a low risk for systemic relapse that are likely to live for many years after the diagnosis of breast cancer.27 There have been reports24 suggesting that adjuvant radiation therapy for breast cancer may increase the risk of lung cancer and angiosarcoma. The risk of sarcoma in the treated volume is likely to be similar with IMRT or standard tech-
niques, but it is possible that second primary lung cancers might be increased by IMRT, especially if the woman is a smoker.27 Therefore, individual assessment of treatment volume goals and longevity of patients with and without radiation therapy is necessary in order to balance the short to medium-term benefits of reducing the volume of critical structures, especially heart and lung, receiving higher radiation dose.

Respiratory gating
Organ motion during the IMRT treatment has been ac-
counted for using real-time position management (RPM; Varian Medical System, Palo Alto, California, USA). The RPM system supports automatic on and off triggering of radiation beam during the treatment. The marker position approximates identical and in-phase alignment of breast and marker motion. Due to breathing motion, the PTV may move outside the external contour as defined on the planning CT and result in a geographic miss of the target. Al-
though the geometric uncertainties and intra fraction move-
ment are taken into account on PTV margin, but the breast is a superficial organ and often the CTV will extend to the skin surface. In these cases, the restriction of the PTV to 3 mm from the skin surface will not provide an adequate mar-
gin for intra-fraction breathing motion.29, 30 The main con-
cern would be the CTV being under-dosed. In order to use gating, the PTV motion must be in phase with the breathing cycle or must at least be able to be predicted from the breathing cycle using technology such as RPM. Conformal blocking and breath-hold techniques can essentially eliminate the heart from the primary beams. Historically, whole heart doses up to 30 Gy were reasonably well tolerated.34-36

Conclusion
IMRT for breast cancer treatment is feasible. In comparison to 3DCRT, IMRT reduced the maximum dose to the target volume, and dose to OAR was reduced too. However, 3DCRT technique was superior in terms of low dose volume of normal tissue, integral dose, and treatment time. Consequences of these low doses would have to be weighed against the benefits of reducing high doses on individual patient selection basis. With the use of breath-hold gated technique in IMRT, it can further improve the target coverage and reduction of doses to the heart, lung, and LAD. SIB tech-
nique could reduce the overall treatment duration by about one week.

Competing interests
The authors declare that they have no conflicts of interest. The authors alone are responsible for the content and writing of the paper.

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